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 Dy^{3+} ion has 5 unpaired electrons but because of a large orbital contribution its effective magnetic moment is 10.5 BM, substantially higher than the spin only value of 5.9 BM. The very short electronic relaxation time of Dy^{3+} means that it has little effect on T_1 but can act as an effective T_2 agent. Advantages over iron oxide particles include improved tolerance and more rapid injection with the prospect of differentiating ischemic tissue from that with normal perfusion. However, similar diagnostic information might be obtained using cheaper, more well established Gd³⁺ complexes.

3.2.1.5 Coordination Compounds as Paramagnetic MRI Contrast Agents

The design of coordination compounds for use as paramagnetic MRI contrast agents presents a particular challenge to the coordination chemist. In order to develop a successful agent it is necessary to reconcile several conflicting requirements. The biological requirement is for a compound with low toxicity combined with suitable biodistribution and pharmokinetic behaviour. Toxicity is a particular issue since relatively large doses are required for an MRI contrast agent to be effective, typically in the range $0.1-0.3 \text{ mmol kg}^{-1}$. This makes it particularly important that the metal is not readily released from the ligand as this would allow binding to serum proteins or other *in vivo* complexing agents. Transfer of the metal in this way would result in a loss of control over metal ion toxicity and biodistribution. Rather the complex should remain intact and be excreted completely and rapidly following the imaging procedure. This requires the complex to be thermodynamically stable and kinetically inert. Suitable modification of ligand structure might then be used to optimise biodistribution and pharmokinetic behaviour.

The basic requirements for an effective contrast agent are that it should have a high magnetic moment, accommodate at least one water molecule in the first coordination sphere of the metal ion and that the coordinated water should undergo rapid exchange with bulk water. In order to attain a high magnetic moment it is necessary to choose high spin metal ions with a large number of unpaired electrons. Such complexes have little or no crystal field stabilisation energy, a property typically resulting in labile behaviour. This labile behaviour is useful in being associated with rapid water exchange. However, the presence of a vacant binding site for water in the complex provides a potential pathway for initiating ligand dissociation. Complexes in which the metal coordination sphere is completely saturated by the ligand so that aquation is blocked would be more inert. Thus the requirements for an effective contrast agent appear to be at odds with those of a complex with suitable in vivo properties. Since complex stability in vivo cannot be attained by using kinetically inert metal ions, stability must be attained largely through the thermodynamics of complex formation. Complexes with very high stability constants are needed. This in turn implies polydentate ligands of suitable structure and with donor atom types chemically well matched to the metal ion. In the case of lanthanide ions such as Gd^{3+} , for example, hard oxygen donor atoms would be preferred for

compatibility with the hard metal centre. The ligand also needs to be anionic as this will promote binding to the metal cation and, if an anionic complex is formed, interactions with outer sphere water will be increased, improving relaxivity. However, charged complexes may be less acceptable in terms of their *in vivo* effects as mentioned in Section 3.2.1.9. Careful selection of the ligand structure can allow the stability of the metal ligand complex to be improved without reducing the lability of coordinated water. As an example a relatively rigid backbone, which requires the ligand donor atoms to occupy locations close to those which will be occupied in the complex, should give a more stable complex than a corresponding ligand with a non-rigid backbone. The more rigid ligand is said to be 'preorganised' in that the structural arrangement of the ligand atoms needs to change little in forming the complex (Figure 8). This reduces the energy penalty associated with complex formation which arises from necessary changes in ligand structure.



Not Preorganised



3.2.1.6 Choice of Metal

As indicated in the preceding discussion the metal ions of particular interest for MRI contrast agent applications include high spin $d^5 \text{ Fe}^{3+}$, high spin $d^5 \text{ Mn}^{2+}$, $f^7 Gd^{3+}$ and $f^5 Dy^{3+}$ (Table 1). The high magnetic moment and long electronic relaxation time of Gd^{3+} make it the most widely used ion in MRI applications. Compared to Gd^{3+} the smaller ionic radius of Mn^{2+} leads to a shorter metalproton distance for coordinated water which to some extent offsets the smaller magnetic moment of Mn^{2+} . The long electronic relaxation time of Mn^{2+} is also an attractive feature but this metal ion shows cardiovascular toxicity at low doses limiting its utility in MRI applications. Iron, in the form of Fe^{3+} , is a d⁵ ion like Mn^{2+} but without the cardiovascular toxicity. In MRI applications Fe^{3+} is typically used in the form of insoluble iron oxide particles which are neither coordination compounds in the usual sense nor solution species. There has been some interest in Dy^{3+} as a T_2 agent since its very short electronic relaxation time leads to its having a negligible effect on T_1 but the high magnetic moment is effective in reducing signal intensity from its effect on T_2 . A Dy³⁺ complex has been tested in humans for identifying ischemic regions in heart and kidney. However, although the use of Dy^{3+} complexes offers interesting possibilities, in general they may not prove competitive with more familiar and medically established Gd^{3+} agents.

3.2.1.7 Choice of Ligand

The ability to provide very high thermodynamic stability, access of water to an inner sphere binding site and allow rapid exchange without compromising stability are important factors in the choice of ligand for MRI applications. Since lanthanide ions, particularly Gd^{3+} , are the metal ions most commonly used in MRI applications anionic hard donor ligands represent an obvious choice. In particular the polyaminepolycarboxylic acid proligand diethylene-triamine pentaacetic acid (**3a**, dtpaH₅ or DTPA¹) and its derivatives (**3b–e**) show strong binding to Ln^{3+} ions through having 'hard' oxygen donor atoms, being polydentate (so stabilising the complexes through the chelate effect) and being able to achieve the high coordination numbers required by Ln^{3+} ions in a 1:1 ligand/metal complex. The well-known proligand edtaH₄ (**4**) is less well suited than dtpaH₅ for Ln^{3+} binding since it offers a maximum coordination number of only 6 in a 1:1 ligand/metal complex. Thus edta⁴⁻ alone cannot saturate the coordination sphere of a lanthanide ion which might typically

¹Very often ligand abbreviations are written in upper case ignoring acidic hydrogen atoms so that ethylenediamine tetra-acetic acid is often referred to as EDTA. However, this can create problems in accurately writing formulae. Under this definition, to be accurate, the formula of the dicalcium salt of ethylenediamine tetra-acetic acid has to be written Ca₂(EDTA-4H) because four H⁺ ions have been lost in forming the complex. To avoid this situation, in this book a lower case text abbreviation is also used which includes ionisable hydrogen in the formula of the proligand, hence edtaH₄ and Ca₂(edta) for the compound containing $2Ca^{2+}$ and $edta^{4-}$. The abbreviation edta simply represents the core of the molecule with hydrogen removed as neutral H atoms. The upper case acronyms are also used in the usual less formal manner often seen in literature, but not in the construction of formulae representing the actual composition of compounds.